

Towards catheter tracking and data-based catheter steering

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Abstract—Minimally invasive surgery (MIS) is an important approach for reducing injuries of the body, allowing faster recovery and healing, and is considered to be safer than open surgeries. Especially for the cardiovascular operations, catheter based diagnosis and therapy are becoming more popular these days. This paper presents an approach of tendon-driven catheter steering by using a joint probability density based catheter model. For tracking the catheter in a 3D rigid mockup, a Qualisys motion tracking system is used. The catheter steering is evaluated in simulation on a mesh generated from the real CT image data.

I. EXPERIMENTAL SETUP

The setup used for pose estimation of ablation catheter is shown in Figure 1. An RFA tendon-driven ablation catheter (EndoSense SA) is used which is placed inside a 3D rigid aorta mock-up. Due to the light reflection and refraction, optical tracking of the objects inside the plastic mock-ups is difficult. Moreover, self-occlusion is another challenge of the object tracking for the normal stereo cameras. Therefore, a near-infrared motion tracking system is used: five Qualisys Oqus-300 near-infrared cameras are placed around the mock-up and six reflective markers are attached on the catheter, which are arranged in an equidistant of 2.7 cm. Since the plastic mock-up is almost transparent for the near-infrared cameras, the system detects the markers more effectively and the self-occlusion problem can be solved by increasing the number of the cameras.

II. METHOD

Due to the compliance of the catheter material and unknown internal friction and associated internal load, the precise position control of tendon-driven catheter is still challenging and being studied by a number of groups, e.g. Kesner et al. [1] analyzed the catheter performance limitations of friction and backlash, and proposed the model-based motion compensation method for the position control of the cardiac catheters. Loschak et al. [2] presented a kinematics-based closed-loop control for a 4 DOFs intracardiac echocardiography catheters. In this paper, we provide a data-driven method for the position control of an ablation catheter tip (3 DOFs) that does not require the internal information of tendon driven catheters.

Figure 2 illustrates the rotate and bend actions of a catheter distal section as well as the reachable position (workspace) of the catheter tip. The yellow, red and green points represent the catheter tip C , bending point B and distal base point

A respectively. The red dash line is the rotation axis of the catheter. Bending the catheter distal section in one direction, the trajectory of the catheter tip is an arc curve. According to the rotational symmetry, the shapes of the bended catheter distal section are the same in any rotation angle. Therefore, learning the catheter shape by applying the bend and rotate actions, the workspace of the catheter tip can be represented as a bowl shape surface, the shaded surface drawn in Figure 2.

During training, the joint probability distribution (JPD) [3] is learned:

$$p(\alpha_t, \theta_t, r_t, d_t) \quad (1)$$

There are four components in the training data. α_t is the current shape of the catheter distal section, which is composed by the positions of catheter interpolated knots, includes catheter tip point, catheter base point and catheter bend point. θ_t represents the current bending angle of the catheter, r_t represents the current rotation angle of the catheter and d_t is the current push distance of the catheter handle. By applying the actions of bend and rotate, the next state of the catheter and the applied actions can be learned as well.

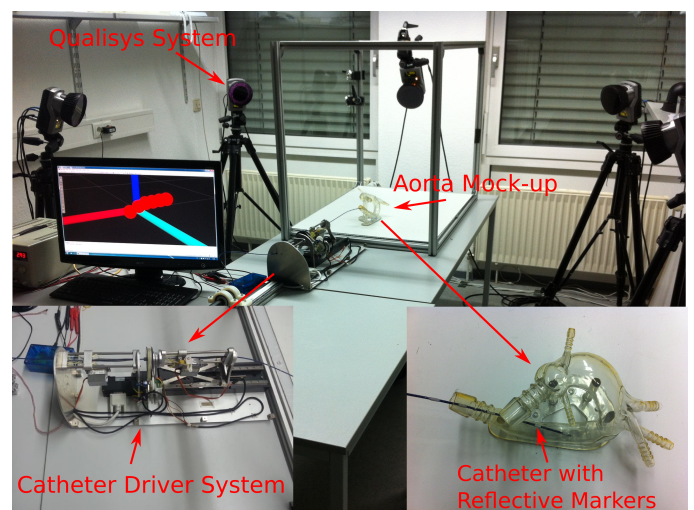


Fig. 1. Visualization of the experimental setup used for pose estimation of catheter with reflective markers inside 3D aorta mock-up

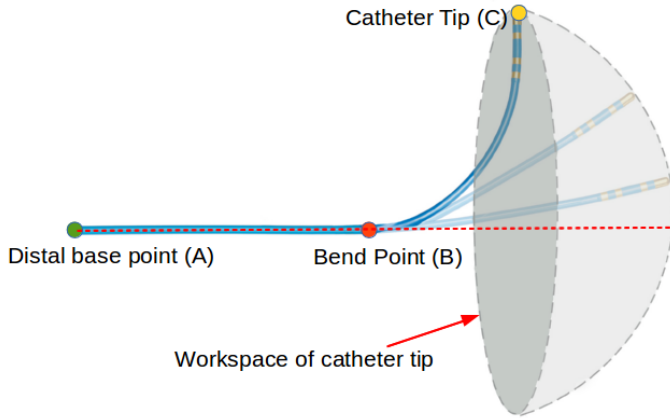


Fig. 2. The catheter steering mechanism and the corresponding bowl shaped catheter tip workspace.

Therefore, the JPD model is represented:

$$p(\alpha_{t+1}, \theta_{t+1}, r_{t+1}, d_{t+1}, \alpha_t, \theta_t, r_t, d_t, \delta_d, \delta_r) \quad (2)$$

Since the tendon-driven catheter is used, the bend action is represented by a displacement of the catheter handle δ_d and δ_r represents rotate action.

In the test, based on the current catheter shape α_t and the every available actions δ_d^*, δ_r^* , the workspace of the catheter tip can be estimated based on the model.

$$\mathbb{E} [p_{t+1}^* | \alpha_t, \theta_t, r_t, d_t, \delta_d^*, \delta_r^*] \quad (3)$$

p_{t+1}^* is the workspace of the catheter tip. Therefore, The crossing point between the planned trajectory and catheter tip workspace can be calculated as the reference position and the corresponding actions are the actions for steering the catheter. Further details are given by Yu et al. [4].

III. RESULTS

Before estimating the catheter pose, the accuracy of the camera system is evaluated by a simple experiment. In the test, two reflective markers are mounted on a rigid bar with a distance of 30 cm to each other. The bar is moved in the testbed area and the markers are detected by the Qualisys system. The distance between the two markers is captured by the camera system in 720 different image frames, which is the estimated distance. The standard deviation of the real distance and the estimated distance of these two markers is calculated, which reaches $0.4213mm$.

Since the aorta mesh is given in a simulation coordinate system, whereas the catheter is captured in the camera coordinate system, a registration step is required to transform the catheter into simulation coordinate system. For calculating the registration matrix, seven reflective markers are attached on the feature positions of 3D real aorta mock-up. By registering the detected feature points from real aorta mock-up to the virtual aorta mock-up in simulation, the catheter pose can be presented in the simulation environment as Figure 3 shows. The six reflective markers which are attached on the ablation catheter are detected and presented as the red dots in the aorta

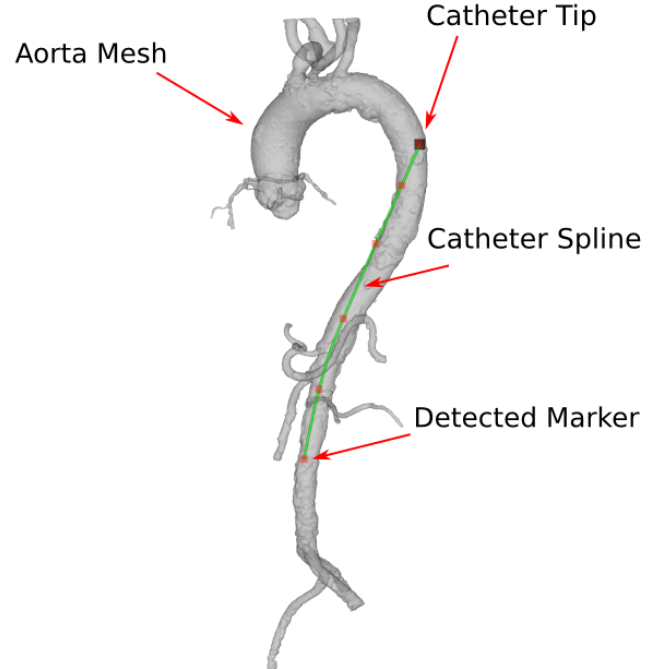


Fig. 3. The pose estimation using Qualisys system: Catheter spline is shown in green, all six of the reflective markers are shown with red dot.

mesh. The green curve is the catheter shape which is calculated by the B-spline curve fitting method.

For evaluating the catheter steering, an autonomous trajectory following experiment is conducted by using a catheter simulator. The simulator includes both a 3D aorta mesh representing the environment and a simulated catheter. For reducing the risk of catheter steering in the cardiovascular system, a trajectory for the catheter tip in the aorta main branch is planned, which keeps largest distance to the detected calcification areas from the real preoperative data. The catheter is inserted into the aorta mesh with 2mm translation steps, based on the catheter steering algorithm, the corresponding actions are generated and the catheter tip is steered towards the trajectory autonomously. Figure 4 shows the planned trajectory and the catheter tip position during the trajectory following test. The mean Euclidean distance from the catheter tip to the trajectory is 4.09mm.

Due to the interaction between the catheter and the aorta vessel has not been included into the model yet, the catheter tip could not follow the planned trajectory smoothly. Therefore in the near future, we will focus on extending our model with the catheter-aorta interaction. In addition to this, safe trajectory following in a real 3D experimental setup (shown in Figure 1) by using the Qualisys system and a catheter drive system will be realized.

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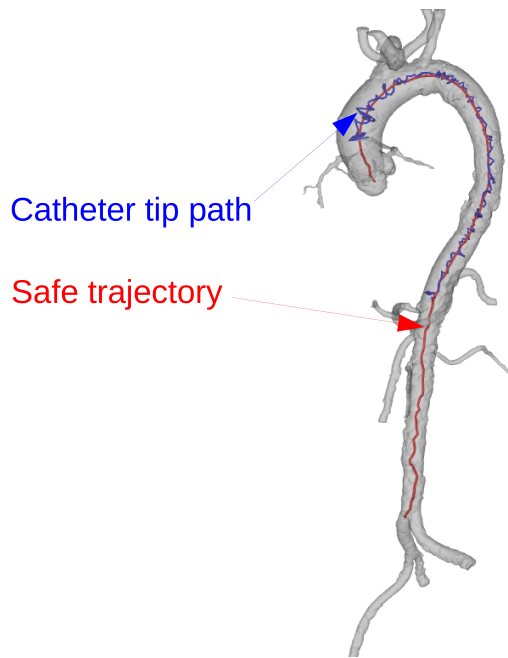


Fig. 4. The result of the catheter trajectory following experiment. The red curve represents the planned trajectory for the catheter and the blue curve is the followed path of the catheter tip.

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